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(54) **Polymer blends for use in making medical devices including catheters and balloons for dilatation catheters**

Polymermischung zum Gebrauch in Herstellung von medizinischen Geräten einschliesslich Kathetern und Ballonen für Dilatationskatheter

Mélange de polymères pour utilisation dans la fabrication d'articles médicaux y compris de cathéters et de ballons pour cathéters de dilatation

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Description**BACKGROUND OF THE INVENTION****Field of the Invention**

[0001] This invention relates generally to a novel polymer blend that can be extruded, molded, or otherwise formed into articles of manufacture having certain desired characteristics. As examples, the polymer blend of the invention can be processed to form medical catheters and more particularly concerns a balloon material for medical balloon dilatation catheters made from blends of a first crystalline polymer component, and a second softening polymer component. The balloon material also includes a third compatibilizing polymer component. While the invention herein relates generally to polymer blends, it will be discussed in terms of preferred end uses in medical devices such as catheters and dilatation balloons. The subsequent discussion is not meant to be limiting and is by way of examples and preferred uses.

Description of Related Art

[0002] Catheters are well known for their usefulness in medical applications, and in particular angioplasty procedures, for opening blood vessels or other passageways in the body that may be blocked by obstructions or stenosis. Dilatation catheters generally are formed from thin, flexible tubing having an inflatable balloon at or near a distal tip of the tubing that can be inflated with fluid pressure, which is communicated to the balloon through a lumen of the tubing. In a typical angioplasty procedure, the balloon dilatation catheter is passed through the vasculature to the location of a stenosis in an artery, and the balloon is inflated to a predetermined size and shape to open the blocked artery.

[0003] It is desirable for balloons of balloon dilatation catheters to be capable of inflating to a diameter of typically five to six times their uninflated diameter, in order to be able to open an obstructed vessel. Other desirable properties of balloons for such balloon dilatation catheters include strength, softness, flexibility and a thin, low, profile, which properties are important for achieving the performance characteristics of folding in an uninflated state, tracking, crossing and re-crossing the area of the obstruction or stenosis in a vessel in an uninflated state. In addition, properties of burst strength, compliance and fatigue increasingly have been important in the continuing effort to create thinner, lower profile balloons for balloon dilatation catheters with an ability to track, cross and re-cross increasingly narrow passages in obstructed vessels. For purposes of this description, the ability to cross is defined as the ability of a balloon of a balloon dilatation catheter to pass through a stenosis; the ability to re-cross is defined as the ability of the balloon of a balloon dilatation catheter to pass through a stenosis more than once, or to pass through more than one stenosis; and the ability to track is defined as the ability of balloon of a balloon dilatation catheter to pass over a guidewire through the tortuous curves of the vasculature, while it is being guided to and from the location of a stenosis.

[0004] Polymeric materials that have been used for making medical devices, catheters, dilatation catheters, and balloons for balloon dilatation catheters include polyethylene, polyolefins, polyvinyl chloride, polyester, polyimide, polyethylene terephthalate (PET), polyamides, nylon, polyurethane, and the like. Balloons made of soft polyolefin or ethylene copolymers typically can be folded, and track and cross well, so that the materials often can be used more than once, and can be used to cross multiple lesions. However, such balloons also commonly have high balloon compliance and low burst strengths, with rated burst pressure of about 80,000-90,000 NT/M² (about 8-9 atm), and a mean burst pressure of about 100,000-150,000 NT/M² (about 10-15 atm). Balloons made from polyethylene terephthalate commonly are stronger, with a higher rated burst pressure of about 140,000-180,000 NT/M² (about 14-18 atm), and a mean burst pressure of about 180,000-250,000 NT/M² (about 18-25 atm). However, dilatation catheter balloons made of PET generally are stiff, cannot be folded and re-folded readily, and are susceptible to acquiring defects during mechanical handling. Dilatation catheter balloons made of PET also are susceptible to pin-hole failures that can cause jet-streaming of pressurized fluid within an artery, and can lead to a dissection of the artery. As a result, to reduce the likelihood of pin-hole failures, clinical applications of balloons made of this type of material generally have been limited to thicker balloons that commonly are limited to a single use and to crossing a single lesion.

[0005] Examples of prior art compositions that may be suitable in forming medical devices such as catheters, dilatation catheters, and balloon materials for use in angioplasty procedures include U.S. Patent No. 4,753,980 (Deyrup); U.S. Patent No. 4,172,859 (Epstein); U.S. Patent No. 5,091,478 (Saltman); U.S. Patent No. 5,306,246 (Sahatjian et al.); U.S. Patent No. 4,254,774 (Boretos); U.S. Patent No. 4,964,409 (Tremulis); and U.S. Patent No. 5,017,325 (Jackowski et al.), all of which are incorporated herein by reference. These references are presented by way of example only and are not intended to be exhaustive of the prior art.

[0006] It would be desirable to provide a polymeric blend for balloons for balloon dilatation catheters with a combination of the best features of the softer balloon materials and the stronger balloon materials, including good flexibility, folding, track, cross and re-cross capability, with a thin, low-profile, a high resistance to fatigue, low compliance, and

high burst strength, with a lower susceptibility to defects resulting from mechanical handling, and a lower susceptibility to pin-hole defects, compared with balloons made from polyethylene terephthalate.

SUMMARY OF THE INVENTION

[0007] Briefly, and in general terms, embodiments of the present invention provide for a catheter and/or balloon material formed from a blend of polymeric components that has surprisingly high-rated burst and mean burst pressure, and has low compliance and excellent fatigue resistance, along with excellent folding and performance characteristics, such as track, cross and re-cross, allowing for construction of dilatation catheter balloons with the ability to cross multiple lesions.

[0008] Particular embodiments of the invention accordingly provide for a catheter and/or balloon material formed from a blend composition of a first crystalline polymeric component and a second softening polymeric component. While the first and second polymeric components essentially are incompatible in that these components are immiscible and do not normally bond together well, a third compatibilizing agent is added to the balloon material that helps to strengthen the interface between the two incompatible materials, and to facilitate blending of the first two polymeric components.

[0009] The first polymeric component generally consists of about 10-95% by weight of the total blend composition, and in one preferred embodiment can be a polyester prepared from the group of dicarboxylic acids selected from aromatic dicarboxylic acids, having from 8 to 14 carbon atoms, and aliphatic dicarboxylic acids, having from 2 to 12 carbon atoms, and at least one glycol selected from the group consisting of glycols having the formula $\text{HO}(\text{CH}_2)_n\text{OH}$, where n is an integer from 2 to 10, neopentyl glycol and cyclohexane dimethanol. In an alternative embodiment, the first polymeric component can be a branched or straight chain polyamide having a molecular weight of at least about 5000. The second polymeric component generally consists of about 5-90% by weight of the total blend composition, is selected to have a Shore hardness less than 75 D, and preferably less than 55 D, and is selected from the group consisting of ethylene copolymers, polyolefins having a density less than 0.93, polyester block copolymers and polyamide block copolymers. The third polymeric component generally consists of an amount of a compatibilizing ethylene copolymer that is less than about 2.5% by weight of the total balloon material blend, and that preferably is about 0.25% to about 2.5% by weight of the total balloon material blend, and that has the formula $\text{E}/\text{X}/\text{Y}$ where E is ethylene; X is an α , β -ethylenically unsaturated monomer derived from at least one of vinyl acetate, alkylacrylate, alkylmethacrylate, alkyl vinyl ether, carbon dioxide, sulfur dioxide, or mixtures thereof, where the alkyl groups contain 1-12 carbon atoms; and Y is an α , β -ethylenically unsaturated monomer containing a reactive group that will form a covalent bond with the first polymeric component. Alternatively, suitable catheter and/or balloon materials can be prepared that contain up to about 20% by weight of the third polymeric component.

[0010] The first polymeric component preferably comprises about 60-77% of the total blend composition, and in a preferred embodiment is selected from the group consisting of polyethylene-terephthalate, polybutylene-terephthalate, glycol modified polyethylene-terephthalate, 1,4-cyclohexylene dimethylene terephthalate/isophthalate copolymer, linear homopolymer esters derived from aromatic dicarboxylic acids and glycols of the general formula $\text{HO}(\text{CH}_2)_n\text{OH}$ where n is an integer from 2 to 10. In a preferred embodiment of the invention, the second polymeric component is a softening ethylene copolymer comprising about 23-40% by weight of the total blend composition, and contains ethylene and at least one other monomer selected from the group consisting of α , β -ethylenically unsaturated monomers, carbon monoxide, and sulfur dioxide. In one particularly preferred embodiment, the softening ethylene copolymer has the formula $\text{E}'\text{X}'$ or $\text{E}'\text{X}'\text{Y}'$, where E' is ethylene, and is about 60-85% by weight of the ethylene copolymer, and where X' is about 15-40% by weight of the ethylene copolymer, and X' is selected from the group consisting of methylacrylate, ethylacrylate, propylacrylate, butylacrylate, and mixtures thereof, and Y' , if present, is an α , β -ethylenically unsaturated monocarboxylic acid, di-acid or anhydride comprising about 0.5-15% by weight of the ethylene copolymer. Examples of Y' include but are not limited to acrylic acid, methacrylic acid, fumaric acid and maleic anhydride. Where one of the X' or Y' monomers is an acid-containing moiety, the polymer can also be at least partially neutralized with an ion selected from the group of sodium, potassium, zinc, lithium, calcium, and ammonium. In a preferred embodiment, in the third polymeric component, X is selected from the group consisting of vinyl acetate, methylacrylate, butylacrylate, and methyl vinyl ether, Y is an α , β -ethylenically unsaturated monomer containing a reactive group selected from the group consisting of epoxide, maleic anhydride, isocyanate, or oxazoline. In one preferred embodiment, Y is selected from the group consisting of glycidyl acrylate, glycidyl methacrylate, and epoxide-containing copolymerizable monomers. In one currently particularly preferred embodiment, in the third polymeric component, E is ethylene, and is 67% by weight of the compatibilizing ethylene copolymer; X is selected from the group of methylacrylate, ethylacrylate, and butylacrylate, and is about 15-30% by weight of the compatibilizing agent; and Y is selected from the group consisting of glycidyl acrylate and glycidyl methacrylate, and is about 8% by weight of the compatibilizing agent.

[0011] These and other aspects and advantages of the invention will become apparent from the following detailed description of the preferred embodiments.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0012] The present invention relates to a polymer blend having certain characteristics generally desirable in medical devices. The polymer blend described herein is particularly suitable for use in forming medical products such as catheters, dilatation catheters, and, preferably, balloon material, for use with catheters.

[0013] While dilatation catheter balloons made of soft polyolefin or ethylene copolymer materials generally have good performance characteristics, such balloons also commonly have high balloon compliance and low burst strength. Dilatation catheter balloons made from strong polymeric materials such as polyethylene terephthalate have higher rated burst pressure and mean burst pressure, but generally are stiff, cannot readily be folded and re-folded, are susceptible to acquiring defects from mechanical handling, and are susceptible to pin-hole failures that can seriously injure the vasculature of a patient. While the embodiments discussed herein refer generally to balloon materials, it is to be understood that the invention relates to catheters, as well, which have the polymer blends as described.

[0014] According to one aspect therefore the invention may be embodied in a balloon material for balloon dilatation catheters with a combination of the best features of the softer balloon materials and the stronger balloon materials, including high burst strength, low compliance, good flexibility, high resistance to fatigue, the ability to fold, track, cross and re-cross well, and with a lower susceptibility to defects through mechanical handling, and a lower susceptibility to pin-hole defects, compared with balloons made from polyethylene terephthalate. The balloon material is formed from a blend of three polymeric components, comprising a strong polymeric component and a softening polymeric component that are generally incompatible with each other, and a compatibilizing polymeric component that forms a covalent bond with one of the first two polymeric components, and prevents the first two polymeric components from separating when formed as a balloon for a balloon dilatation catheter.

[0015] The first polymeric component, component A, preferably is a relatively strong crystalline polymer, preferably comprising about 60-77% of the total blend composition, although blend compositions comprising as little as 10% or as much as 95% of the total blend composition also may be suitable. In one currently preferred embodiment, component A comprises polyethylene terephthalate, but also can comprise other polyesters, or polyamides. Other polyesters which can be used as component A include polyesters prepared from an aromatic dicarboxylic acid having from 8 to 14 carbon atoms and at least one glycol, including those having the formula $\text{HO}(\text{CH}_2)_n\text{OH}$, where n is an integer of 2 to 10, neopentyl glycol and cyclohexane dimethanol. The dicarboxylic acid may also be an aliphatic dicarboxylic acid having from 2 to 12 carbon atoms. Examples of other suitable polyesters include, but are not limited to, polybutylene-terephthalate (PBT), glycol-modified polyethylene terephthalate (PETG), 1,4-cyclohexylene dimethylene terephthalate/isophthalate copolymer and other linear homopolymer esters derived from aromatic dicarboxylic acids and glycols of the general formula $\text{HO}(\text{CH}_2)_n\text{OH}$, where n is an integer from 2 to 10. Such aromatic dicarboxylic acids include isophthalic, bibenzoic, naphthalene-dicarboxylic including the 1,5-; 2,6-; and 2,7-naphthalenedicarboxylic acids; 4,4'-diphenylenedicarboxylic acid; bis(p-carboxyphenyl) methane; ethylene-bis-p-benzoic acid; 1,4-tetramethylene bis(p-oxybenzoic) acid; ethylene bis(p-oxybenzoic) acid; 1,3-trimethylene bis(p-oxybenzoic) acid; and 1,4-tetramethylene bis(p-oxybenzoic) acid. Preferred glycols include ethylene glycol; 1,3-trimethylene glycol; 1,4-tetramethylene glycol; 1,6-hexamethylene glycol; 1,8-octamethylene glycol; 1,10-decamethylene glycol; 2,2-dimethyl-1,3-propane diol; 1,3-propylene glycol; 1,4-butyleneglycol; neopentyl glycol and cyclohexane dimethanol.

[0016] Polyamides which are suitable for use as component A include branched or straight chain polyamides having a molecular weight of at least 5000, and commonly referred to as nylons; produced by condensation of equimolar amounts of a saturated dicarboxylic acid containing from 4 to 12 carbon atoms with a diamine, in which the diamine contains from 4 to 12 carbon atoms. Examples of suitable polyamides include, but are not limited to, nylons such as polyhexamethylene adipamide (nylon 6,6), polyhexamethylene azelaamide (nylon 6,9), polyhexamethylene sebacamide (nylon 6,10), polyhexamethylene dodecanoamide (nylon 6,12), nylon 6, nylon 11, and nylon 12. Other polyamides that can be suitable include polyamide block copolymers such as those sold under the trade name "PEBAX" by the AtoChem Company; polyamides including polyamides produced by the ring opening of lactams such as polycaprolactam, polylauric lactam, poly-11-amino-undecanoic acid, and bis(paraaminocyclohexyl) methane dodecanoamide; and polyamides prepared by the copolymerization or terpolymerization of such polymers. The polyamides preferably have a melting point in excess of 200 °C (392 °F).

[0017] The second polymeric component, component B, is selected to be a softening polymer, preferably comprising about 23-40% by weight of the total balloon material composition, although blends of the balloon material comprising as little as 5% of component B and as much as 90% of the total blend composition also may be suitable. In a currently preferred embodiment, component B comprises a softening polymer component having a Shore hardness less than 75 D, and preferably less than 55 D, and preferably is an elastomeric ethylene copolymer selected from the group of α , β -ethylenically unsaturated monomers, carbon monoxide (CO), sulfur dioxide (SO₂). Component B is most preferably an elastomeric ethylene copolymer having the formula $\text{E}'\text{X}'$ or $\text{E}'\text{X}'\text{Y}'$, where E' is ethylene and comprises about 60-85% by weight of the ethylene copolymer, X' is acrylate or methacrylate monomer, comprising about 15-40% of the ethylene copolymer,

and Y', if present YT, is an α , β -ethylenically unsaturated monocarboxylic acid, di-acid or anhydride comprising about 0.5-15% by weight of the ethylene copolymer. Examples of Y' include but are not limited to acrylic acid, methacrylic acid, fumaric acid and maleic anhydride. Other polymeric materials that may be suitable for use as component B include, but are not limited to, polyester block copolymers (containing one or more of the following glycols) comprising hard segments of polyethylene-terephthalate or polybutylene-terephthalate, and soft segments of polyether such as polyethylene glycol, polypropylene glycol or polytetramethylene glycol ethers, such as those available under the trade-name "HYTREL" from the E.I. DuPont & DeNemours Co. Long-chain glycols, which can be used to prepare such copolyester polymers, include poly(alkylene oxide), glycols in which the alkylene group has 2-10 carbon atoms, such as poly(ethylene oxide) glycol, poly(1,2- and 1,3- propylene oxide) glycol, poly(tetramethylene oxide) glycol, poly(pentamethylene oxide) glycol, poly(hexamethylene oxide) glycol, poly(heptamethylene oxide) glycol, poly(octamethylene oxide) glycol, poly(nonamethylene oxide) glycol, and poly(1,2-butylene oxide) glycol, random or block copolymers of ethylene oxide and 1,2-propylene oxide, and poly-formals prepared by reacting formaldehyde with glycols, such as propylene glycol, or mixtures of glycols, such as a mixture of tetramethylene and pentamethylene glycols, and glycols formed from dicarboxymethyl acids of poly(alkylene oxides); polyetherimide esters such as those produced under the tradename "LOMOD" by the General Electric Company; polyesters available from Dutch State Mines under the trade name "ARNITEL"; polyamide block copolymers, such as those available from the AtoChem Company under the trade-name "PEBAX"; and polyolefins having a density less than 0.93, including elastomeric ethylene-propylene copolymers, linear low density polyethylene (LLDPE), and linear low density polyethylene (LLDPE) including maleic anhydride.

[0018] The most preferred ethylene copolymers which can be used as component B include, but are not limited to, ethylene/methylacrylate/sulfur dioxide (E/MA/SO₂), ethylene/butylacrylate/carbon monoxide (E/BA/CO), ethylene/methylacrylate (E/MA), ethylene ethylacrylate (E/EA), ethylene/butylacrylate (E/BA), ethylene/vinylacetate (E/VA), ethylene/methacrylic acid (E/MAA or E/AA), ethylene/butylacrylate/methacrylic acid (E/BA/MAA or E/BA/AA), ethylene/methylacrylate/methacrylic acid (E/MA/MAA or E/MA/AA), ethylene/butylacrylate/maleic anhydride (E/BA/Manh) or ethylene/methylacrylate/maleic anhydride (E/MA/Manh). Where one of the α , β -ethylenically unsaturated monomers is an acid-containing moiety, the polymer can be partially neutralized with an ion such as Na⁺, K⁺, Zn⁺⁺, Li⁺, Ca⁺⁺, NH₄⁺, or the like. The acid groups in the unsaturated mono-carboxylic acid are neutralized from 0-80% by at least one metal ion selected from the group consisting of sodium, zinc, magnesium, calcium, potassium, and lithium. The third polymeric component, component C, is an ethylene copolymer that functions as a compatibilizing agent or surfactant, in that it forms a covalent bond with the first polymeric component, and blends compatibly with the second polymeric component. Component C comprises from less than about 2.5% of the total blend composition provided that the compatibilizing ethylene copolymer is included in the polymer blend, having the formula E/X/Y, where E is about 67%, X is about 25%, and Y is about 8% by weight of the compatibilizing ethylene copolymer, and

E is ethylene,

X is an α , β -ethylenically unsaturated monomer derived from at least one of alkylacrylate, alkylmethacrylate, alkyl vinyl ether, carbon dioxide, sulfur dioxide, or mixtures thereof, where the alkyl groups contain 1-12 carbon atoms, such as vinyl acetate, methylacrylate, butylacrylate, and methyl vinyl ether. X can, for example, be a moiety derived from at least one of alkyl acrylate, alkyl methacrylate, alkyl vinyl ether, carbon monoxide, sulfur dioxide, or mixtures thereof. More specifically, X can, for example, consist of 0-35 weight percent of a moiety derived from at least one alkyl acrylate, alkyl methacrylate, or mixtures thereof where the alkyl groups contain 1-8 carbon atoms.

[0019] Y is an α , β -ethylenically unsaturated monomer containing a reactive group, such as epoxide, maleic anhydride, isocyanate, or oxazoline, for example, that forms a covalent bond with said first polymeric component. In one preferred embodiment, Y is selected from the group consisting of glycidyl methacrylate and glycidyl acrylate, maleic anhydride, and isocyanato-ethylmethacrylate.

[0020] In one currently preferred embodiment the first polymeric component of the balloon material blend comprises about 70-77% by weight polyethylene terephthalate; about 23-30% by weight of component B, which comprises an ethylene copolymer having the formula E'X', where E' is ethylene, and is about 75% by weight of the ethylene copolymer, and X' is selected from the group of ethylene methylacrylate, ethylene ethylacrylate, ethylene propylacrylate, and ethylene butylacrylate, and is about 25% by weight of the ethylene copolymer; and from about 0.25% to about 2.5% by weight of component C, which is an ethylene copolymer having the formula EXY, where E is ethylene, and is 67% by weight of component C; X is selected from the group of ethylene acrylate and ethylene methylacrylate, and is about 25% by weight of component C; and Y is selected from the group consisting of glycidyl methacrylate, glycidyl ethylacrylate, and glycidyl butylacrylate, and is about 8% by weight of component C. The second polymeric component, component B, most preferably is an elastomeric ethylene copolymer selected from the group consisting of ethylene/methylacrylate, ethylene/ethylacrylate, ethylene/butylacrylate, ethylene/methylacrylate/maleic anhydride, ethylene/ethylacrylate/maleic anhydride, and ethylene/butylacrylate/maleic anhydride; and the third polymeric component, component C, is most preferably an ethylene acrylate ester where X is selected from methyl acrylate, ethyl acrylate and

butyl acrylate, and Y is selected from the group consisting of glycidyl acrylate and glycidyl methacrylate.

[0021] In addition, in a preferred aspect of the invention, the balloon material advantageously can be irradiated using ionizing radiation from an electron beam, gamma rays, ultraviolet light, or a molecular beam, to significantly alter the properties of the balloon material to provide improved balloon performance such as higher burst pressures. For example, where the balloon material was subjected to an electron beam of about 10-100 MRads and energies of 100-200,000 keV, higher burst strengths and higher fatigue strengths were obtained from the balloon material.

[0022] The balloon materials embodying the invention provide dilatation catheter balloons with the ability to cross multiple lesions, good track, cross, and folding characteristics, low compliance with rated burst pressures of about 100,000-150,000 NT/M² (about 10-15 atm), and mean burst pressures of about 140,000-200,000 NT/M² (about 14-20 atm). Balloons made from the balloon material described also typically have a lower susceptibility to defects through mechanical handling than does polyethylene terephthalate. When exposed to ionizing radiation to toughen the balloon material, the fatigue and burst strengths are substantially increased, to provide rated burst pressures of 120,000-140,000 NT/M² (12-14 atm) or greater mean burst pressures of 190,000-200,000 NT/M² (19-20 atm), and a compliance of about .02 X 10⁻⁵ - .03 X 10⁻⁵ mm/NT/M² (about .02-.03 mm/atm).

Example 1 (not part of the invention)

[0023] A polymer blend containing 80 weight % PET Traytuf 9506C (polyethylene terephthalate) manufactured by the Shell Company, and 20 weight % EEA (ethylene ethylacrylate) DPDA 6182 manufactured by the Union Carbide Company, was produced by compounding in a twin screw extruder set for low shear conditions. The PET and EEA were mixed in a weight ratio of 80/20. The PET/EEA mixture was loaded into the hopper of the compounder. The barrel temperatures were set to 210 °C (410 °F) in zone 1, 254 °C (490 °F) in zones 2 and 3, and 249 °C (480 °F) in zone 4 and at the head of the barrel, the screw speed was maintained at 942 radians per minute (150 revolutions per minute), and the material was pelletized. Balloon tubing having an inner diameter of 0.46 mm (0.018 inches) and an outer diameter of 0.91 mm (0.036 inches) was extruded using the 80/20 PET/EEA blend. The 80/20 PET/EEA blended material was dried. The barrel and die temperatures of the extruder were set, with zone 1 at 199 °C (390 °F), zone 2 at 249 °C (480 °F), zone 3 at 260 °C (500 °F), and the clamp, die 1 and die 2 at 265 °C (510 °F). The melt temperature of the blend was 301 °C (574 °F). Examination with a scanning electron microscope of a portion of the blend before extrusion into balloon tubing showed that the EEA formed spherical particles with a diameter greater than 1µm with poor interfacial adhesion within the PET matrix. A section of the extruded balloon tubing also was examined with a scanning electron microscope, showing that the EEA formed tubules in the extruded balloon tubing that pulled out of the PET matrix.

Example 2

[0024] The blend of PET and EEA from Example 1 was compounded and blended with 2% of the total blend composition by weight of a third component, E/EA/GMA, as a compatibilizer, available as Lotader AX8660 from the AtoChem Company. Examination with a scanning electron microscope of a portion of the blend before extrusion into balloon tubing showed that the EEA formed a much better dispersion with better interfacial adhesion within the PET matrix, with little or no particle pull-out from the PET matrix. A section of the extruded balloon tubing made from the blend also was examined with a scanning electron microscope, showing that the EEA formed no tubules in the extruded balloon tubing, and that the dispersed particles of EEA were well adhered to the PET matrix. The material had a burst pressure of about 344,750 NT/M² (3.4 atm; 50 psi) higher than in Example 1.

Examples 3-10

[0025] Balloon material blends also were formed using PET available as Traytuf 9506C from the Shell Company, with a tensile strength of 4 X 8 X 10⁷ NT/M² (7000 psi; 476 atm) (non-oriented), and of 69-83 X 10⁶ NT/M² (10000-12000 psi; 681-817 atm) (oriented), an elongation of 400-500% (after yield), a flexural modulus of 3 X 4 - 4 X 14 X 10⁹ NT/M² (500,000-600,000 psi), and a melting point of 257 °C (494.6 °F). EEA available as DPDA 6182 from the Union Carbide Company was used in Examples 3-5 and 8-10, with a tensile strength of 1 X 6 X 10⁷ NT/M² (2300 psi), elongation of 670%, a flexural modulus of 4 X 4 X 10⁷ NT/M² (6400 psi), a melt index of 1.5, a Durometer of 91A, a melting point of 85 °C (185 °F), a density of 0.93 gms/cm³ and a Vicat Softening index of 64. EMAC available as TC130 from the Exxon Company was used in Examples 6 and 7, with a tensile strength of 8 X 3 X 10⁷ NT/M² (1200 psi), an elongation of 1600%, a flexural modulus of 2 X 3 X 10⁷ (3300 psi), a melt index of 20, a Durometer of 85A, a melting point of 79° C, a density of 0.94 gms/cm² and a Vicat Softening index of 50. Lotryl 24MA005 (EMA) from the AtoChem Company was used as the softening component in Example 10, with a tensile strength of 2 X 0 X 10⁷ NT/M² (2910 psi), elongation of 700%, a melt index of 0.5, a Durometer of 84A, a melting point of 70 °C (158 °F), and a Vicat

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Softening index of 43. Lotader AX8660 (67% E, 25% EA, 8% GMA) from the AtoChem Company was used as the compatibilizing agent in Examples 4-10, with a tensile strength of $3 \times 5 \times 10^6$ NT/M² (509 psi), an elongation of 700%, a melt index of 6.0, a Durometer of 60A, a melting point of 63 °C (145 °F), and a Vicat Softening index of 34.

[0026] The blend compositions of Examples 3-10 are listed in Table I below, and were compounded under the compounding conditions noted in Table II and were extruded under the tubing extrusion conditions noted in Table III.

TABLE I

Example	PET %	EEA %	EMAC %	Lotryl %	Lotader %
3	60	40	-	-	-
4	78.4	19.6	-	-	2
5	76	19	-	-	5
6	78.4	-	19.6	-	2
7	76	-	19	-	5
8	68.8	29.5	-	-	1.7
9	59.1	39.4	-	-	1.5
10	70	-	-	28	2

TABLE II

Example	3	4	5	6	7	8	9	10
T1 °C (°F)	210 (410)	210 (410)	210 (410)	204.4 (400)	204.4 (400)	204.4 (400)	204.4 (400)	135 (275)
T2 °C (°F)	254.4 (490)	248.9 (480)	248.9 (480)	248.9 (480)	248.9 (480)	232.2 (450)	232.2 (450)	248.9 (480)
T3 °C (°F)	254.4 (490)	248.9 (480)	248.9 (480)	254.4 (490)	254.4 (490)	251.7 (485)	251.7 (485)	279.4 (535)
T4 °C (°F)	248.9 (480)	260 (500)	260 (500)	268.3 (515)	268.3 (515)	260 (500)	260 (500)	290.6 (555)
Thead °C (°F)	248.9 (480)	260 (500)	260 (500)	268.3 (515)	268.3 (515)	260 (500)	260 (500)	290.6 (555)
Rad/min (rev/min)	942.5 (150)	942.5 (150)	942.5 (150)	942.5 (150)	942.5 (150)	942.5 (150)	942.5 (150)	942.5 (150)
Dry °C (°F)	148.9 (300)	93.3 (200)	93.3 (200)	93.3 (200)	93.3 (200)	93.3 (200)	93.3 (200)	93.3 (200)

TABLE III

Example	3	4	5	6	8	10
T1 °C (°F)	198.9 (390)	204.4 (400)	204.4 (400)	187.8 (370)	204.4 (400)	207.2 (405)
T2 °C (°F)	248.9 (480)	248.9 (480)	248.9 (480)	221.1 (430)	248.9 (480)	251.7 (485)
T3 °C (°F)	260 (500)	265.6 (510)	265.6 (510)	248.9 (480)	260 (500)	254.4 (490)
Tclamp °C (°F)	265.6 (510)	265.6 (510)	265.6 (510)	248.9 (480)	260 (500)	254.4 (490)

TABLE III (continued)

Example	3	4	5	6	8	10
Tdie1 °C (°F)	256.6 (510)	256.6 (510)	256.6 (510)	248.9 (480)	260 (500)	254.4 (490)
Tdie2 °C (°F)	256.6 (510)	256.6 (510)	256.6 (510)	248.9 (480)	260 (500)	260 (500)
I.D. mm (in)	.457 (.018)	.508 (.020)	.508 (.020)	.508 (.020)	.508 (.020)	.508 (.020)
O.D. mm (in)	.914 (.036)	1.02 (.040)	1.02 (.040)	1.02 (.040)	1.02 (.040)	1.02 (.040)
Dry °C (°F)	65.6 (150)	65.6 (150)	65.6 (150)	65.6 (150)	65.6 (150)	65.6 (150)

Example 11

[0027] In Example 11, a blend composition was compounded according to the method of Example 1. Tubing was extruded with an inner diameter of 4.57 mm (0.18 inches), an outer diameter of .914 mm (0.036 inches), and a double wall thickness (DWT) of 0.034 mm (0.00135 inches). The balloon formed from the tubing was subjected to 25 Mrads of radiation, and had a mean burst pressure of $1 \times 72 \times 10^6$ NT/M² (250 psi; 17 atm).

Examples 12-13

[0028] In Examples 12 and 13, a blend composition was compounded according to the method of Example 2. In Example 12, tubing was extruded with an inner diameter of .508 mm (.020 inches) and an outer diameter of 1.02 mm (.040 inches). Balloons were formed with an outer diameter of 3.02 mm (.119 inches), a DWT of .038 mm (.0015 inches), and were subjected to 40 Mrads of radiation and demonstrated higher burst pressures. For example, the balloon formed from the tubing had a mean burst pressure of $1 \times 97 \times 10^6$ NT/M² (285 psi; 19.4 atm). Tubing not subjected to irradiation was formed into a balloon with an outer diameter of 3.04 mm (.1195 inches), a DWT of .037 mm (.00145 inches), and a mean burst pressure of $1 \times 7 \times 10^6$ NT/M² (252 psi; 17.1 atm).

Examples 14-15

[0029] In Examples 14 and 15, a polymer blend containing 90 weight % PET Traytuf 9506C manufactured by the Shell Company, and 10 weight percent of an ionomeric resin of ethylene and methacrylic acid, available under the tradename "SURLYN," manufactured by the DuPont deNemours Company, were blended. The materials were separately dried. Balloon tubing having an inner diameter of .533 mm (.021 inches) and an outer diameter of .826 mm (.0325 inches) was extruded using this 90/10 blend. The barrel and die temperatures of the extruder were set with Zone 1 at 237.8 °C (460 °F), Zone 2 at 251.7 °C (485 °F), Zone 3 at 260 °C (500 °F), die 1 at 271.1 °C (520 °F), die 2 at 271.1 °C (520 °F).

[0030] In Example 14, a balloon was formed and material had a mean burst pressure of $1 \times 4 \times 10^6$ NT/M² (207 psi; 14.1 atm).

[0031] In Example 15, tubing was formed as in Example 13. The tubing was subjected to 20Mrads of radiation. The balloons formed had a mean burst pressure of $1 \times 76 \times 10^6$ NT/M² (255 psi; 17.3 atm).

Claims

1. A polymeric blend material comprising:

60 to 77% by weight of the total blend composition of a first polymeric component selected from the group consisting of polyesters and polyamides, said polyesters being prepared from the group of acids selected from aromatic dicarboxylic acids having from 8 to 14 carbon atoms and aliphatic dicarboxylic acids having from 2 to 12 carbon atoms, and at least one glycol selected from the group consisting of glycols having the formula HO(CH₂)_nOH, where n is an integer from 2 to 10, neopentyl glycol and cyclohexane dimethanol, and said

polyamides being branched or straight chain polyamides having a molecular weight of at least 5000; 23-40% by weight of the total blend composition of a second polymer component having a Shore hardness less than 75 D and said second polymeric component is an ethylene copolymer comprising ethylene and at least one other monomer selected from the group consisting of α,β -ethylenically unsaturated monomers, carbon monoxide and sulfur dioxide; and

less than about 2.5% by weight of the total blend composition of a compatibilizing ethylene copolymer having the formula E/X/Y where

E is ethylene,

X is an α,β -ethylenically unsaturated monomer derived from at least one of alkylacrylate, alkylmethacrylate, alkyl vinyl ether, carbon monoxide, sulfur dioxide, or mixtures thereof, where the alkyl groups contain 1 to 12 carbon atoms, and

Y is an α,β -ethylenically unsaturated monomer containing a reactive group that forms a covalent bond with said first polymeric component,

and wherein the second polymer component and the compatibilizing ethylene copolymer are not identical with the proviso that the compatibilizing ethylene copolymer is included in the polymer blend.

2. The material of claim 1, wherein said first polymeric component is selected from the group consisting of polyethylene-terephthalate, polybutylene-terephthalate, glycol modified polyethylene-terephthalate, 1,4-cyclohexylene dimethylene terephthalate/isophthalate copolymer, linear homopolymer esters derived from aromatic dicarboxylic acids and glycols of the general formula $\text{HO}(\text{CH}_2)_n\text{OH}$ where n is an integer from 2 to 10.

3. The material of claim 1, wherein said first polymeric component is a polyester having glycol segments selected from the group consisting of ethylene glycol; 1,3-trimethylene glycol; 1,4-tetramethylene glycol; 1,6-hexamethylene glycol; 1,8-octamethylene glycol; 1,10-decamethylene glycol; 2,2-dimethyl-1,3-propane diol; 1,3-propylene glycol; 1,4-butylene glycol; neopentyl glycol and cyclohexane dimethanol.

4. The material of claim 1, wherein said second polymeric component is an ethylene copolymer having the formula E'X' or E'X'Y, where

E' is ethylene, and is 60 to 85% by weight of the ethylene copolymer, where

X' is 15 to 40% by weight of the ethylene copolymer, and is selected from the group consisting of methylacrylate, ethylacrylate, propylacrylate, butylacrylate and mixtures thereof, and

Y' is selected from the group consisting of α,β -ethylenically unsaturated monocarboxylic acids, α,β -ethylenically unsaturated dicarboxylic acids, and anhydrides comprising 0.5 to 15% by weight of the ethylene copolymer.

5. The material of claim 1, wherein X is a moiety derived from at least one alkyl acrylate, alkyl methacrylate, or mixtures thereof, where the alkyl groups contain 1-8 carbon atoms.

6. The material of claim 1, wherein Y is an α,β -ethylenically unsaturated monomer containing a reactive group selected from the group consisting of epoxide, maleic anhydride, isocyanate, or oxazoline.

7. The material of claim 1, wherein Y is selected from the group consisting of glycidyl methacrylate, glycidyl acrylate, maleic anhydride, and isocyanato-ethylmethacrylate.

8. The material of claim 1 wherein Y is an α,β -ethylenically unsaturated mono-carboxylic acid which is neutralized at least partially by at least one metal ion selected from the group consisting of sodium, zinc, magnesium, calcium, potassium, and lithium.

9. The material of claim 1, wherein E is ethylene, and is about 67% by weight of the compatibilizing ethylene copolymer; X is selected from the group of methylacrylate, ethylacrylate and butylacrylate, and is about 25% by weight of the compatibilizing ethylene copolymer; and Y is selected from the group consisting of glycidyl acrylate and glycidyl methacrylate, and is about 8% by weight of the compatibilizing ethylene copolymer.

10. The material of claim 1, wherein said material is irradiated.

11. The material of claim 1, wherein said material is irradiated using ionizing radiation generated by any of an electron beam, gamma rays, ultraviolet light, or a molecular beam.

12. The material of claim 1, wherein said material is irradiated by an electron beam in the range of 10-100 Mrads.
13. The material of claim 1, wherein the compatibilizing ethylene copolymer is present in an amount of from 0.25% to 2.5% by weight of the total blend composition.
14. A medical device at least partially formed of a material in accordance with any of the preceding claims.
15. A device as claimed in claim 14 which is a catheter or a balloon formed of the material.

Patentansprüche

1. Polymeres Mischungsmaterial umfassend:

60 bis 77 Gew.-% der gesamten Mischungszusammensetzung einer ersten Polymerkomponente, die aus der Gruppe bestehend aus Polyestern und Polyamiden ausgewählt ist, wobei die Polyester aus der Gruppe von Säuren, die aus aromatischen Dicarbonsäuren mit 8 bis 14 Kohlenstoffatomen und aliphatischen Dicarbonsäuren mit 2 bis 12 Kohlenstoffatomen ausgewählt sind, und mindestens einem Glycol, das aus der Gruppe bestehend aus Glycolen mit der Formel $\text{HO}(\text{CH}_2)_n\text{OH}$, wobei n eine ganze Zahl von 2 bis 10 ist, Neopentylglycol und Cyclohexandimethanol ausgewählt ist, hergestellt sind und die Polyamide verzweigte oder geradkettige Polyamide mit einem Molekulargewicht von mindestens 5.000 sind;

23-40 Gew.-% der gesamten Mischungszusammensetzung einer zweiten Polymerkomponente, die eine Shore-Härte von weniger als 75 D aufweist, und wobei die zweite Polymerkomponente ein Ethylen-Copolymer ist, das Ethylen und mindestens ein anderes Monomer, das aus der Gruppe bestehend aus α,β -ethylenisch ungesättigten Monomeren, Kohlenmonoxid und Schwefeldioxid ausgewählt ist, umfaßt; und weniger als etwa 2,5 Gew.-% der gesamten Mischungszusammensetzung eines kompatibilisierenden Ethylen-Copolymers mit der Formel E/X/Y, wobei

E Ethylen ist,

X ein α,β -ethylenisch ungesättigtes Monomer ist, das von mindestens einem von Alkylacrylat, Alkylmethacrylat, Alkylvinylether, Kohlenmonoxid, Schwefeldioxid oder Mischungen davon abgeleitet ist, wobei die Alkylgruppen 1 bis 12 Kohlenstoffatome enthalten, und

Y ein α,β -ethylenisch ungesättigtes Monomer ist, das eine reaktive Gruppe enthält, die eine kovalente Bindung mit der ersten Polymerkomponente bildet,

und wobei die zweite Polymerkomponente und das kompatibilisierende Ethylen-Copolymer nicht identisch sind, mit der Maßgabe, daß das kompatibilisierende Ethylen-Copolymer in der Polymermischung eingeschlossen ist.

2. Material nach Anspruch 1, wobei die erste Polymerkomponente aus der Gruppe bestehend aus Polyethylenterephthalat, Polybutylenterephthalat, Glycol-modifiziertem Polyethylenterephthalat, 1,4-Cyclohexyldimethylen-terephthalat/isophthalat-Copolymer, linearen Homopolymer-Estern, die von aromatischen Dicarbonsäuren und Glycolen der allgemeinen Formel $\text{HO}(\text{CH}_2)_n\text{OH}$, wobei n eine ganze Zahl von 2 bis 10 ist, abgeleitet sind, ausgewählt ist.

3. Material nach Anspruch 1, wobei die erste Polymerkomponente ein Polyester ist, der Glycol-Segmente aufweist, die aus der Gruppe bestehend aus Ethylenglycol, 1,3-Trimethylenglycol, 1,4-Tetramethylenglycol, 1,6-Hexamethylenglycol, 1,8-Octamethylenglycol, 1,10-Decamethylenglycol, 2,2-Dimethyl-1,3-propandiol, 1,3-Propylenglycol, 1,4-Butylenglycol, Neopentylglycol und Cyclohexandimethanol ausgewählt sind.

4. Material nach Anspruch 1, wobei die zweite Polymerkomponente ein Ethylen-Copolymer ist, welches die Formel E'X' oder E'X'Y aufweist, wobei

E' Ethylen ist und 60 bis 85 Gew.-% des Ethylen-Copolymers darstellt, wobei

X' 15 bis 40 Gew.-% des Ethylen-Copolymers darstellt und aus der Gruppe bestehend aus Methylacrylat, Ethylacrylat, Propylacrylat, Butylacrylat und Mischungen davon ausgewählt ist, und

Y', umfassend 0,5 bis 15 Gew.-% des Ethylen-Copolymers, aus der Gruppe bestehend aus α,β -ethylenisch ungesättigten Monocarbonsäuren, α,β -ethylenisch ungesättigten Dicarbonsäuren und Anhydriden ausgewählt ist.

5. Material nach Anspruch 1, wobei X eine Gruppierung ist, die von mindestens einem Alkylacrylat, Alkylmethacrylat oder Mischungen davon abgeleitet ist, wobei die Alkylgruppen 1-8 Kohlenstoffatome enthalten.
6. Material nach Anspruch 1, wobei Y ein α,β -ethylenisch ungesättigtes Monomer ist, das eine reaktive Gruppe enthält, die aus der Gruppe bestehend aus Epoxid, Maleinsäureanhydrid, Isocyanat oder Oxazolin ausgewählt ist.
7. Material nach Anspruch 1, wobei Y aus der Gruppe bestehend aus Glycidylmethacrylat, Glycidylacrylat, Maleinsäureanhydrid und Isocyanatoethylmethacrylat ausgewählt ist.
8. Material nach Anspruch 1, wobei Y eine α,β -ethylenisch ungesättigte Monocarbonsäure ist, welche mindestens teilweise durch mindestens ein Metallion neutralisiert ist, das aus der Gruppe bestehend aus Natrium, Zink, Magnesium, Calcium, Kalium und Lithium ausgewählt ist.
9. Material nach Anspruch 1, wobei E Ethylen ist und etwa 67 Gew.-% des kompatibilisierenden Ethylen-Copolymers darstellt; X aus der Gruppe von Methylacrylat, Ethylacrylat und Butylacrylat ausgewählt ist und etwa 25 Gew.-% des kompatibilisierenden Ethylen-Copolymers darstellt; und Y aus der Gruppe bestehend aus Glycidylacrylat und Glycidylmethacrylat ausgewählt ist und etwa 8 Gew.-% des kompatibilisierenden Ethylen-Copolymers darstellt.
10. Material nach Anspruch 1, wobei das Material bestrahlt ist.
11. Material nach Anspruch 1, wobei das Material unter Einsatz von ionisierender Strahlung, erzeugt durch irgendeines von Elektronenstrahlen, Gammastrahlen, UV-Licht oder einem Molekülstrahl, bestrahlt ist.
12. Material nach Anspruch 1, wobei das Material durch einen Elektronenstrahl im Bereich von 10 - 100 Mrad bestrahlt ist.
13. Material nach Anspruch 1, wobei das kompatibilisierende Ethylen-Copolmer in einer Menge von 0,25 bis 2,5 Gew.-% der gesamten Mischungszusammensetzung anwesend ist.
14. Medizinische Vorrichtung, die zumindest teilweise aus einem Material nach irgendeinem der vorhergehenden Ansprüche hergestellt ist.
15. Vorrichtung nach Anspruch 14, welche ein aus dem Material hergestellter Katheter oder Ballon ist.

Revendications

1. Matière consistant en un mélange polymère, comprenant :

60 à 77 % en poids de la composition de mélange totale d'un premier constituant polymère choisi dans le groupe consistant en des polyesters et des polyamides, lesdits polyesters étant préparés à partir du groupe d'acides choisis entre des acides dicarboxyliques aromatiques ayant 8 à 14 atomes de carbone et des acides dicarboxyliques aliphatiques ayant 2 à 12 atomes de carbone, et d'au moins un glycol choisi dans le groupe consistant en des glycols répondant à la formule $\text{HO}(\text{CH}_2)_n\text{OH}$, dans laquelle n représente un nombre entier de 2 à 10, le néopentyl-glycol et le cyclohexane-diméthanol, et lesdits polyamides étant des polyamides à chaîne ramifiée ou droite ayant un poids moléculaire d'au moins 5000 ;

23 à 40 % en poids de la composition de mélange totale d'un second constituant polymère ayant une dureté Shore inférieure à 75 D, ledit second constituant polymère étant un copolymère d'éthylène comprenant de l'éthylène et au moins un autre monomère choisi dans le groupe consistant en des monomères à insaturation α,β -éthylénique, le monoxyde de carbone et le dioxyde de soufre ; et moins d'environ 2,5 % en poids de la composition de mélange totale d'un copolymère d'éthylène compatibilisant répondant à la formule E/X/Y dans laquelle

E représente l'éthylène,

X représente un monomère à insaturation α,β -éthylénique dérivé d'au moins un des composés consistant en un acrylate d'alkyle, un méthacrylate d'alkyle, un éther d'alkyle et de vinyle, le monoxyde de carbone, le dioxyde de soufre et leurs mélanges, dans lesquels les groupes alkyle contiennent 1 à 12 atomes de carbone, et Y représente un monomère à insaturation α,β -éthylénique contenant un groupe réactif qui forme une liaison covalente avec ledit premier constituant polymère,

dans laquelle le second constituant polymère et le copolymère d'éthylène compatibilisant ne sont pas identiques, sous réserve que le copolymère d'éthylène compatibilisant soit incorporé au mélange polymère.

2. Matière suivant la revendication 1, dans laquelle le premier constituant polymère est choisi dans le groupe consistant en un polymère de téréphtalate de polyéthylène, un polymère de téréphtalate de butylène, un polymère de téréphtalate d'éthylène modifié avec un glycol, un copolymère 1,4-cyclohexylène-téréphtalate/isophtalate de diméthylène, des esters homopolymères linéaires dérivés d'acides dicarboxyliques aromatiques et de glycols, de formule générale $\text{HO}(\text{CH}_2)_n\text{OH}$ dans laquelle n représente un nombre entier de 2 à 10.
3. Matière suivant la revendication 1, dans laquelle le premier constituant polymère est un polyester comprenant des segments glycol choisis dans le groupe consistant en l'éthylène-glycol ; le 1,3-triméthylène-glycol ; le 1,4-tétraméthylène-glycol ; le 1,6-hexaméthylène-glycol ; le 1,8-octaméthylène-glycol ; le 1,10-décaméthylène-glycol ; le 2,2-diméthyl-1,3-propane-diol ; le 1,3-propylène-glycol ; le 1,4-butylène-glycol ; le néopentyl-glycol et le cyclohexane-diméthanol.
4. Matière suivant la revendication 1, dans laquelle le second constituant polymère est un copolymère d'éthylène répondant à la formule $\text{E}'\text{X}'$ ou $\text{E}'\text{X}'\text{Y}'$, dans laquelle

E' représente l'éthylène, et est présent en une quantité de 60 à 85 % en poids du copolymère d'éthylène,
X' représente 15 à 40 % en poids du copolymère d'éthylène et est choisi dans le groupe consistant en l'acrylate de méthyle, l'acrylate d'éthyle, l'acrylate de propyle, l'acrylate de butyle et leurs mélanges, et
Y' est choisi dans le groupe consistant en des acides monocarboxyliques à insaturation α,β -éthylénique, des acides dicarboxyliques à insaturation α,β -éthylénique, et leurs anhydrides, représentant 0,5 à 15 % en poids du copolymère d'éthylène.
5. Matière suivant la revendication 1, dans laquelle X représente un groupement dérivé d'au moins un acrylate d'alkyle, d'un méthacrylate d'alkyle ou de leurs mélanges, dans lesquels les groupes alkyle contiennent 1 à 8 atomes de carbone.
6. Matière suivant la revendication 1, dans laquelle Y représente un monomère à insaturation α,β -éthylénique contenant un groupe réactif choisi dans le groupe consistant en des groupes époxyde, anhydride maléique, isocyanate et oxazoline.
7. Matière suivant la revendication 1, dans laquelle Y est choisi dans le groupe consistant en le méthacrylate de glycidyle, l'acrylate de glycidyle, l'anhydride maléique et le méthacrylate d'isocyanato-éthyle.
8. Matière suivant la revendication 1, dans laquelle Y représente un acide monocarboxylique à insaturation α,β -éthylénique qui est neutralisé au moins partiellement par au moins un ion métallique choisi dans le groupe consistant en sodium, zinc, magnésium, calcium, potassium et lithium.
9. Matière suivant la revendication 1, dans laquelle E est l'éthylène et représente environ 67% en poids du copolymère d'éthylène compatibilisant ; X est choisi dans le groupe consistant en l'acrylate de méthyle, l'acrylate d'éthyle et l'acrylate de butyle et représente environ 25 % en poids du copolymère d'éthylène compatibilisant ; et Y est choisi dans le groupe consistant en l'acrylate de glycidyle et le méthacrylate de glycidyle et représente environ 8 % en poids du copolymère d'éthylène compatibilisant.
10. Matière suivant la revendication 1, qui est irradiée.
11. Matière suivant la revendication 1, qui est irradiée en utilisant un rayonnement ionisant engendré par n'importe laquelle des sources consistant en un faisceau d'électrons, des rayons gamma, la lumière ultraviolette et un faisceau moléculaire.
12. Matière suivant la revendication 1, qui est irradiée par un faisceau d'électrons dans la plage de 10 à 100 Mrads.
13. Matière suivant la revendication 1, dans laquelle le copolymère d'éthylène compatibilisant est présent en une quantité de 0,25 % à 2,5 % en poids de la composition du mélange totale.
14. Dispositif médical formé au moins partiellement d'une matière suivant l'une quelconque des revendications pré-

cédentes.

15. Dispositif suivant la revendication 14, qui est un cathéter ou ballonnet formé de cette matière.

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